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Efficiency of a Cherenkov based PET module with an array of SiPMs

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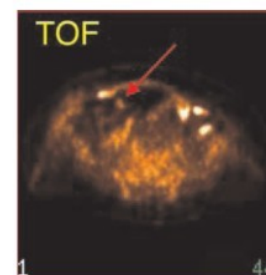
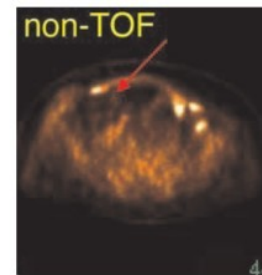
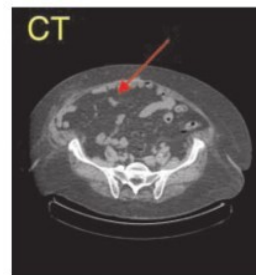
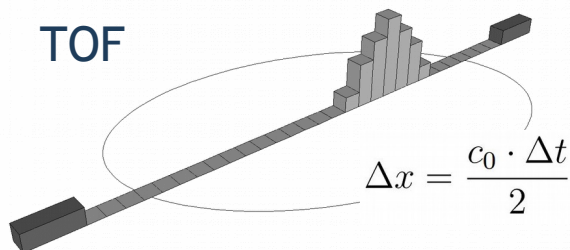
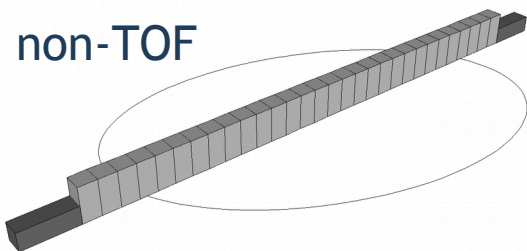
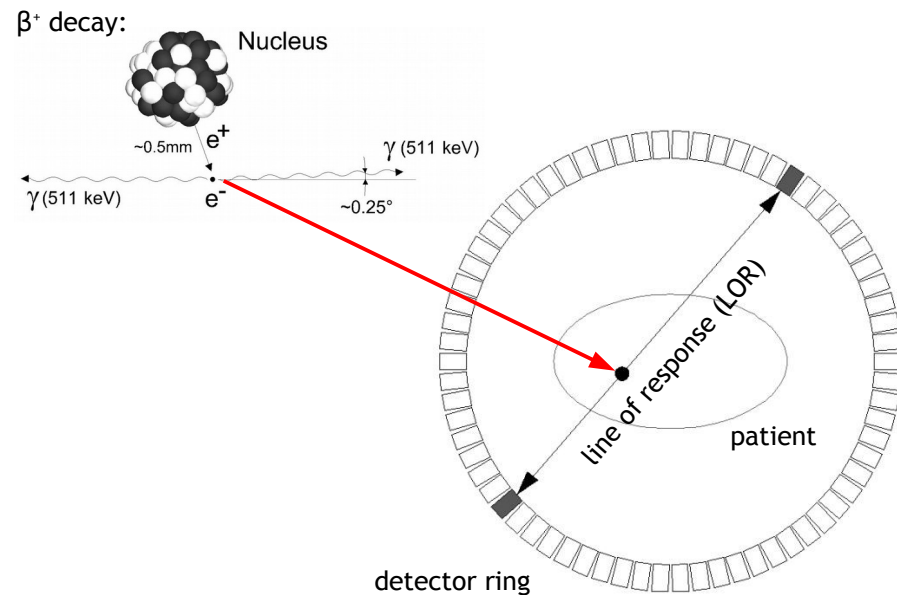
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- Time-of-flight (TOF) positron emission tomography (PET)
- Use of Cherenkov radiation for TOF PET
- Previous experiments
 - microchannel plate photomultipliers (MCP PMT) as photodetectors
 - silicon photomultipliers (SiPM) as photodetectors
- 16 channel Cherenkov PET module
 - measurements of detection efficiency
- Summary

Positron emission tomography

- Positron emission tomography (PET)
 - medical physics modality, enabling in-vivo imaging of biological processes via coincident detection of 511 keV annihilation γ rays
- Time-of-flight (TOF)
 - measurement of arrival times of the two γ can be used to limit the reconstructed position of annihilation
 - improves the quality (contrast-to-noise ratio) of reconstructed images



Philips Gemini TF PET/CT, TOF resolution of 600 ps
[PET Center of Excellence Newsletter, Vol.3 Issue 3 (2006)]

Use of Cherenkov Light in TOF PET

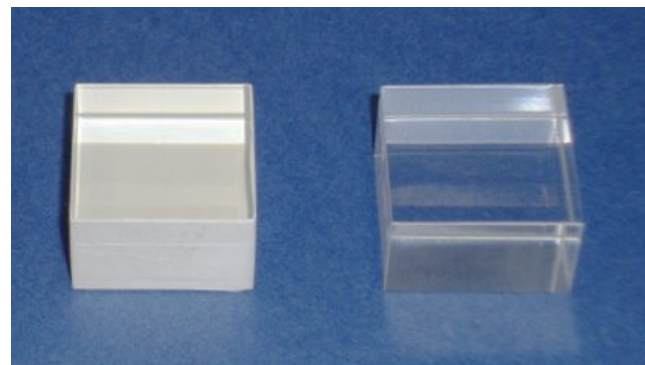
- γ detectors in traditional PET: scintillator crystal + photodetector

	BGO	LSO	LaBr ₃ (Ce)	PbF ₂
Density (g/cm ³)	7.1	7.4	5.1	7.77
$\mu_{511\text{keV}}$ (cm ⁻¹)	0.96	0.87	0.43	1.06
Photofraction for 511 keV (*)	0.41	0.32		0.46
Decay time (ns)	300	40	17	-
Light yield (/511 keV)	3,000	15,000	30,000	10 (‡)

(*) [XCOM: Photon Cross Sections Database]

(‡) in 250-800 nm wavelength interval

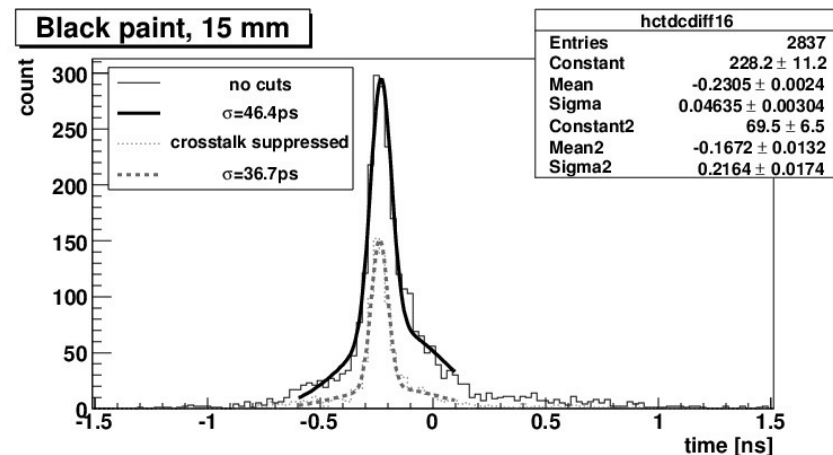
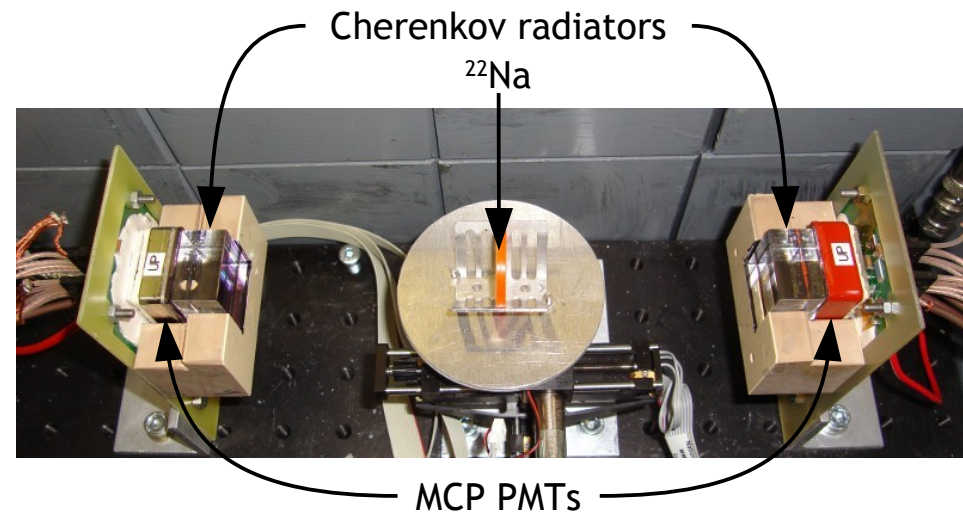
- Lead fluoride (PbF₂) crystal
 - exclusively Cherenkov light produced (prompt)
 - excellent properties for stopping 511 keV annihilation γ
 - excellent light transmission (down to 250 nm)
 - low cost
 - low light yield - single photon detection



Previous results (MCP PMT)

- Two detectors in back-to-back configuration
- Cherenkov radiators
 - 25x25x5 or 25x25x15 mm³ PbF₂
- Photodetectors
 - microchannel plate photomultiplier tubes (MCP PMTs)
 - single photon timing ~ 50 ps FWHM
 - active surface 22.5x22.5 mm²
- TOF (coincidence) resolution:
 - **71 ps FWHM** (5 mm thick, black painted PbF₂)
 - **95 ps FWHM** (15 mm thick, black painted PbF₂)
- Low efficiency ~ 6% (single side)
 - traditional scintillation detectors ~ 30%

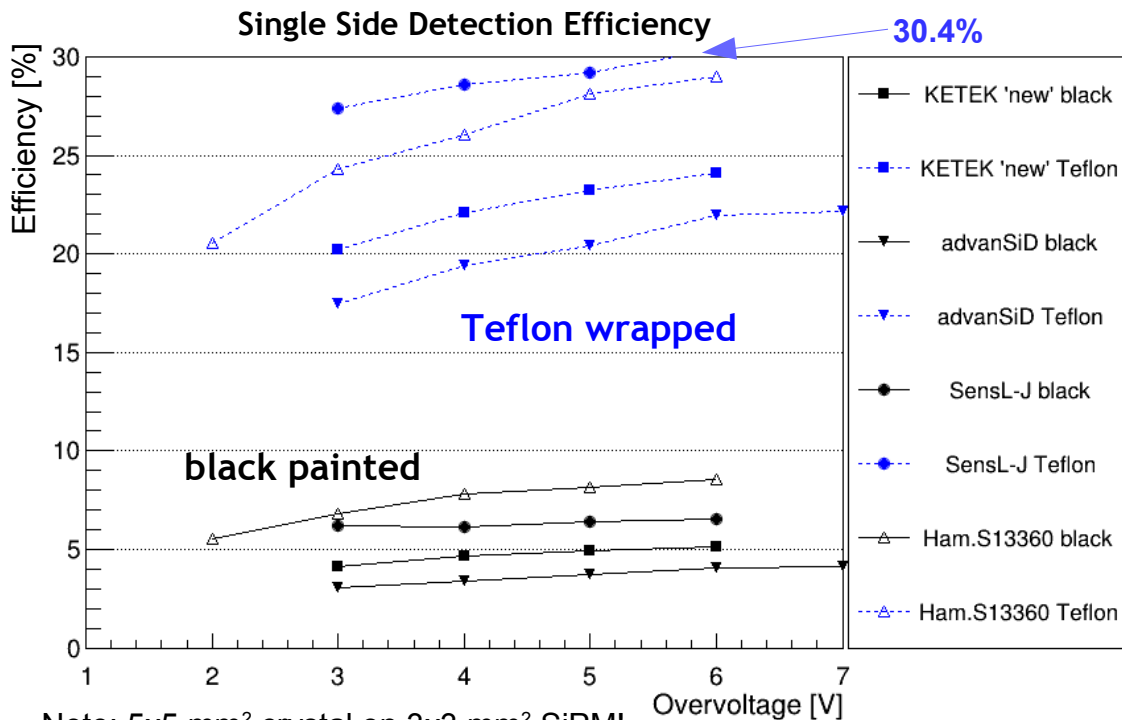
NIM A 654 (2011) 532



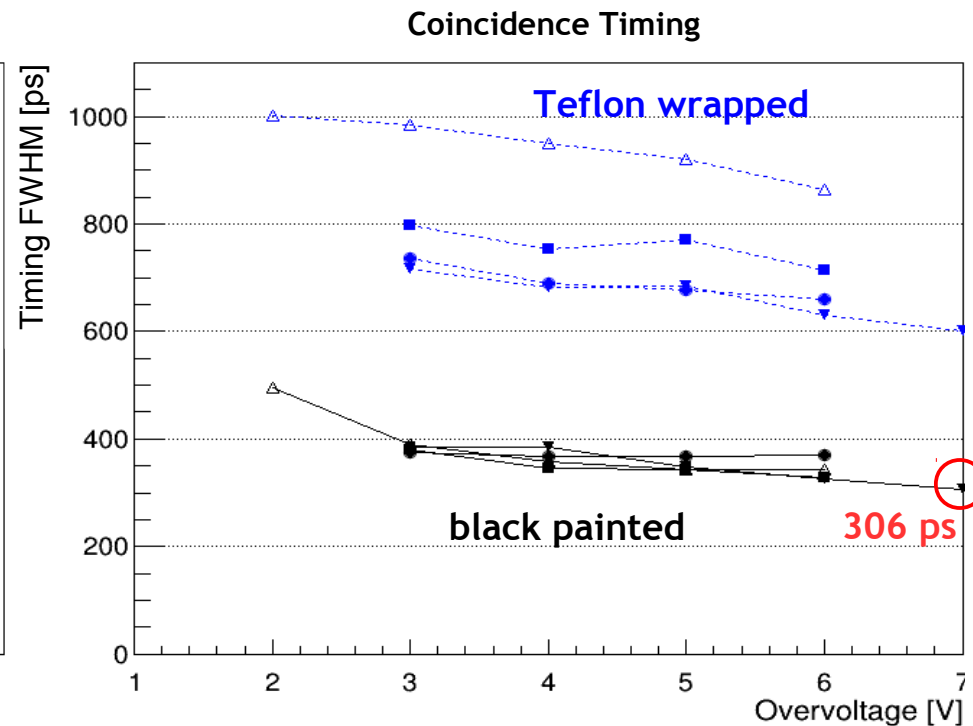
Previous results (SiPM)

- Two detectors in back-to-back configuration
- Cherenkov radiators: $5 \times 5 \times 15 \text{ mm}^3 \text{ PbF}_2$
- Photodetectors: $3 \times 3 \text{ mm}^2$ silicon photomultipliers
 - cooled to -25°C (SiPM dark counts)

- TOF (coincidence time) resolution:
 - 306 ps FWHM (AdvanSiD, black paint)
- Efficiency:
 - 30% single side (SensL-J, Teflon wrapped)

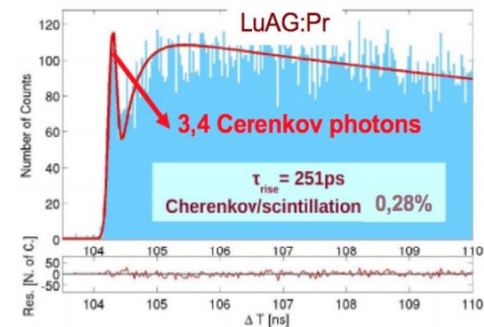


Note: $5 \times 5 \text{ mm}^2$ crystal on $3 \times 3 \text{ mm}^2$ SiPM!

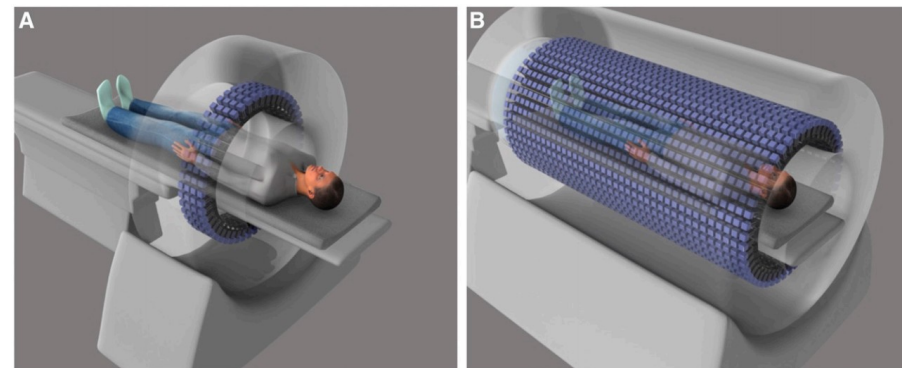


Summary of previous results

- Excellent TOF PET timing achievable using exclusively Cherenkov light:
 - 95 ps FWHM coincidence timing with 15 mm thick PbF_2 ($\sim \gamma$ stopping power of 20 mm of LSO)
 - Cherenkov considered for the goal of 10 ps TOF PET [P. Lecoq]
- Very few (single) photons
 - efficiency an issue
- Silicon photomultipliers
 - Cherenkov PET efficiency competitive to scintillators ($\sim 30\%$ single side)
 - timing an issue (especially with configuration optimized for efficiency)
- Cost of $\text{PbF}_2 \sim 20\%$ of LSO (cost of scintillator $\sim 50\%$ of PET scanner)
 - lower cost PET scanners
 - total-body PET scanners [S. Cherry]
- Our next step
 - PET module, optimized of efficiency and price



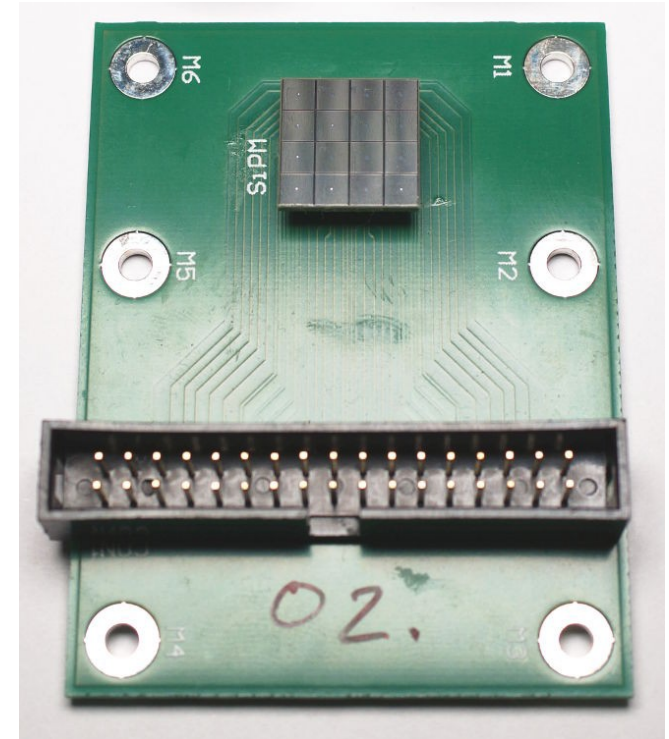
[Lecoq et al., IEEE TRPMS, Vol. 1, No. 6 (2017)]



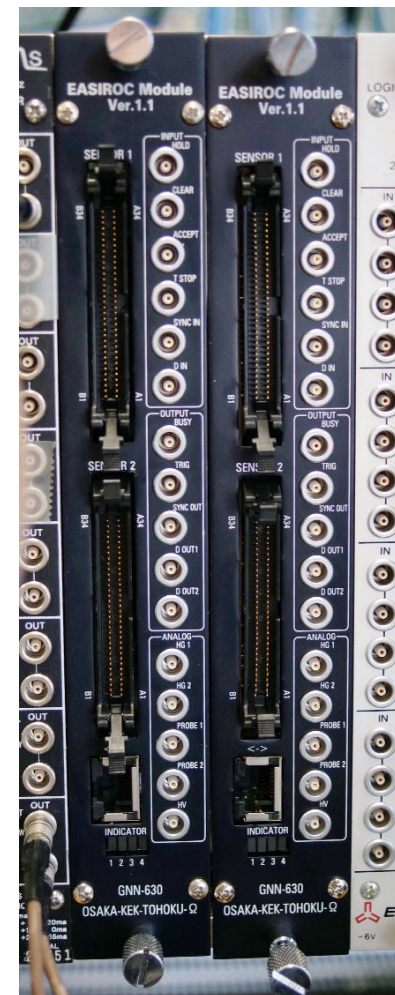
[Cherry et al., The Journal Of Nuclear Medicine, Vol. 59, No. 1 (2018)]

16 channel PET module

- Cherenkov radiators
 - 4x4 array of 3x3x15 mm³ PbF₂
[Shanghai SICCAS High Technology Corporation]
 - white reflector (black paint where noted)
- Photodetectors
 - 4x4 array of 3x3 mm² SiPM
 - Hamamatsu MPPC S13361-3075AS-04
 - 75 μ m pixels (1600 / 3x3 mm²)
 - peak sensitivity ~ 50% PDE @ 450 nm
 - breakdown voltage ~ 53 V
 - dark count ~ 0.5 Mcps (/ 3x3 mm²), crosstalk prob. ~ 7% (overvoltage $V_{ov} = 3$ V)
- Custom connector board
- 3D printed crystal supports
- SiPM bias provided by readout module - EASIROC

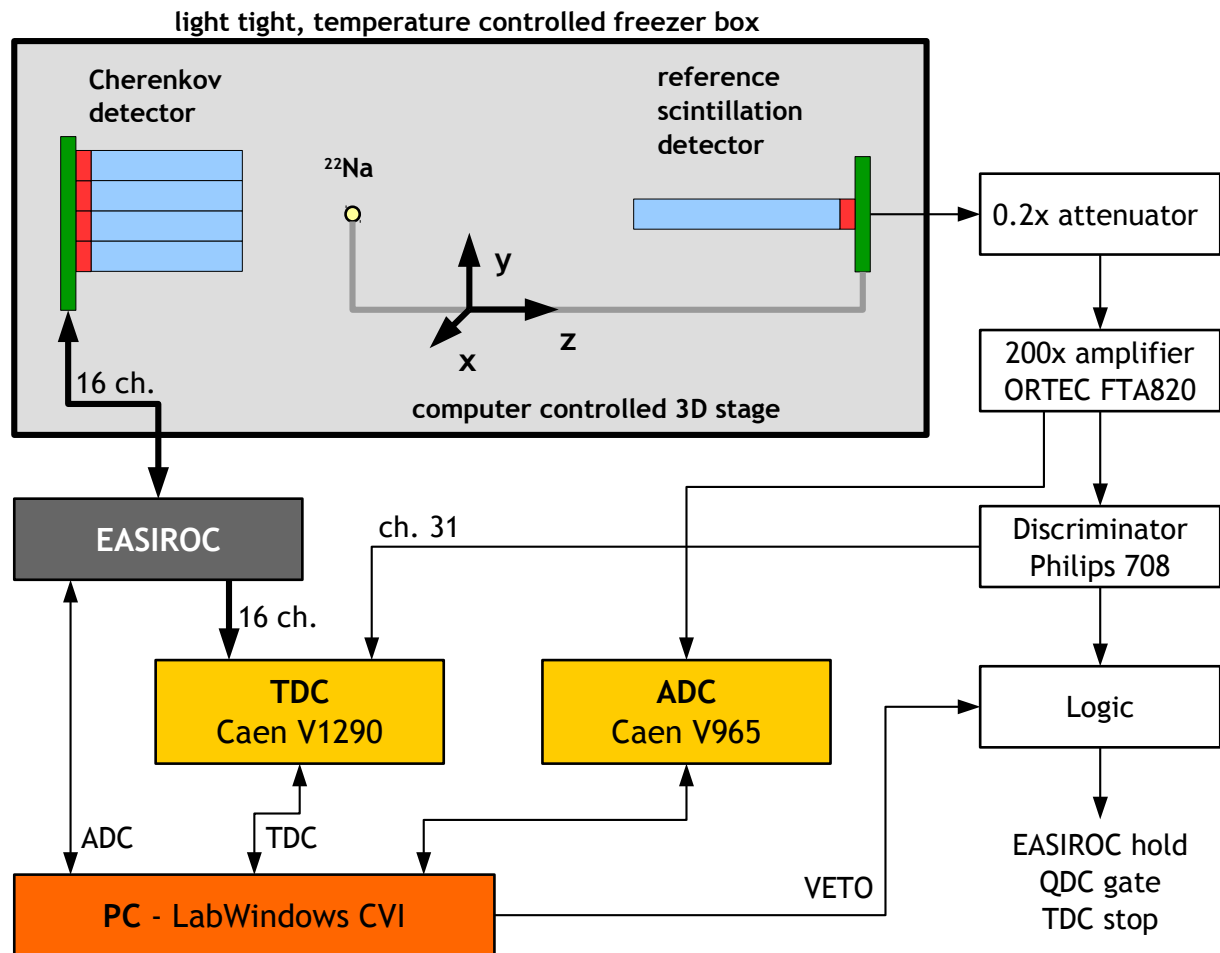


- EASIROC chip [OMEGA group]
 - Extended Analogue Silicon pm Integrated Read Out Chip
 - 32 channel ASIC dedicated to read-out of SiPM detectors
 - Internal input 8-bit DAC for individual SiPM gain adjustment
 - Individually addressable calibration injection capacitance
 - Energy measurement : 14-bit dynamic range
 - Trigger output
- EASIROC module [Osaka, KEK]
 - 2 x 16 channels per module
 - **SiPM bias supply**, adjustable by 4.5V for each channel
 - **ADC**, 12bit, dual range
 - **LVDS trigger** outputs (for external TDC)
 - possibility to perform TDC in FPGA (~ 1ns resolution)
 - Ethernet connection to PC



Experimental setup

- Cherenkov detector:
 - 4x4 array of $3 \times 3 \times 15 \text{ mm}^3$ PbF_2
 - 4x4 array of $3 \times 3 \text{ mm}^2$ SiPM
- Reference detector
 - $3 \times 3 \times 30 \text{ mm}^3$ LYSO scintillator
 - $3 \times 3 \text{ mm}^2$ SiPM
- Annihilation γ source
 - ^{22}Na point source ($D = 0.3 \text{ mm}$)
 - activity = 0.6 MBq
- Temperature: -25°C (SiPM dark counts)

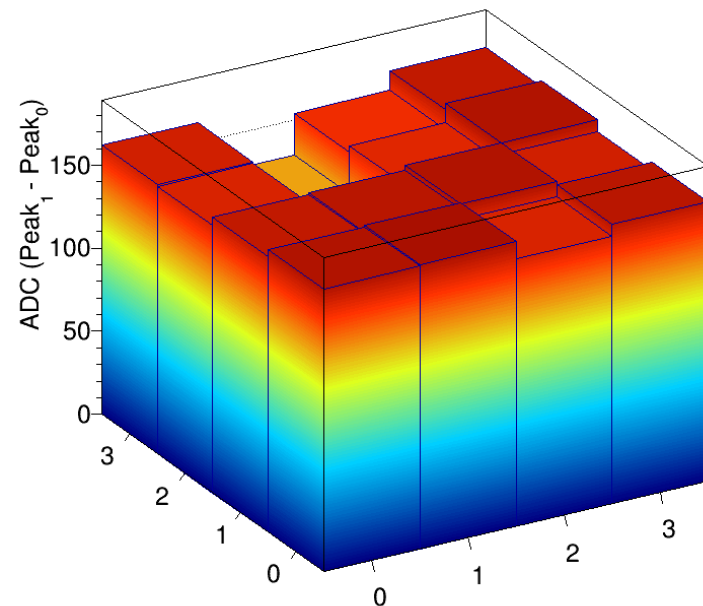
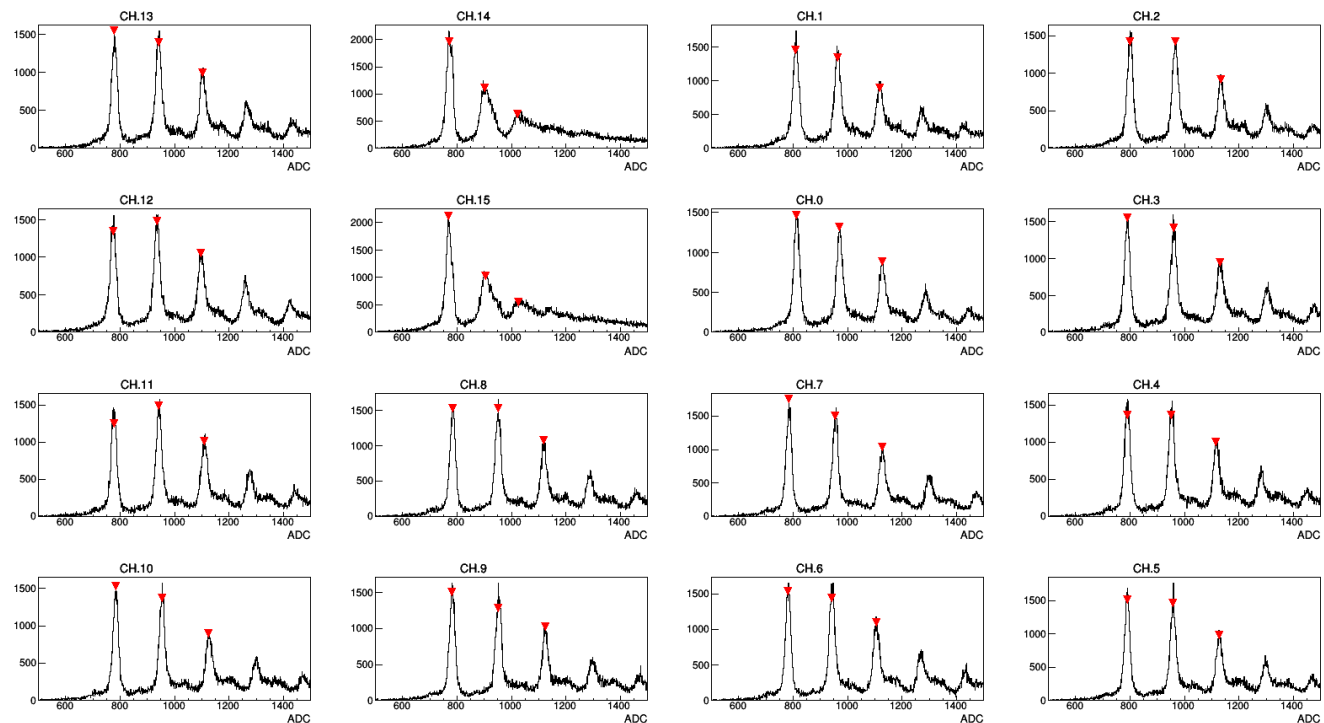


Laser calibration

- Laser illumination instead of reference scintillation detector
 - ~1 mm laser spot scanned over each SiPM array channel center (w/o PbF₂ crystals)
 - gain ~ (ADC 1 p.e. peak) - (ADC noise peak)
 - adjusted for each channel

Channel

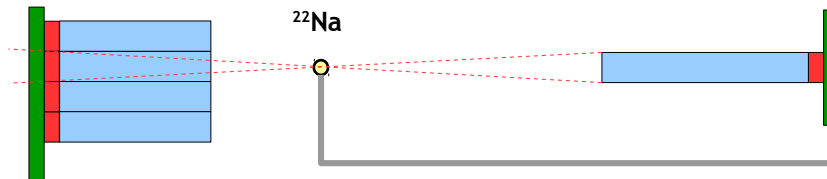
13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5



laser; T = +25°C; V_{ov} = 5 V

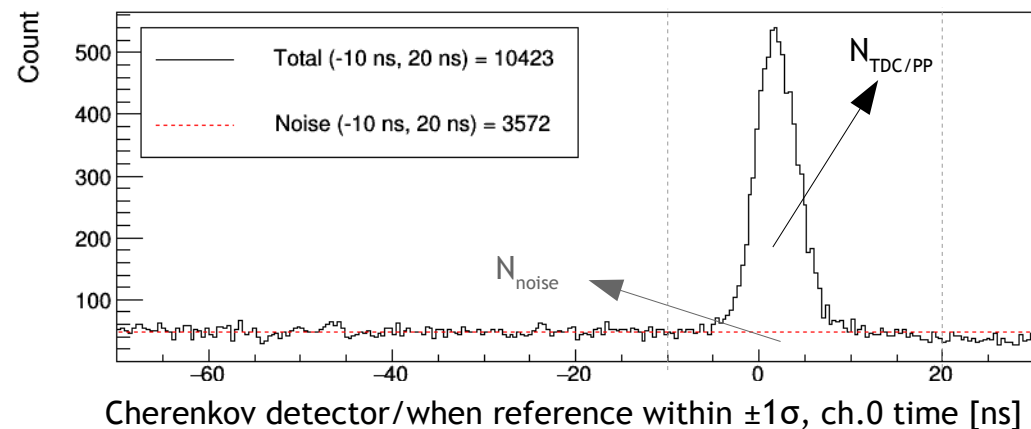
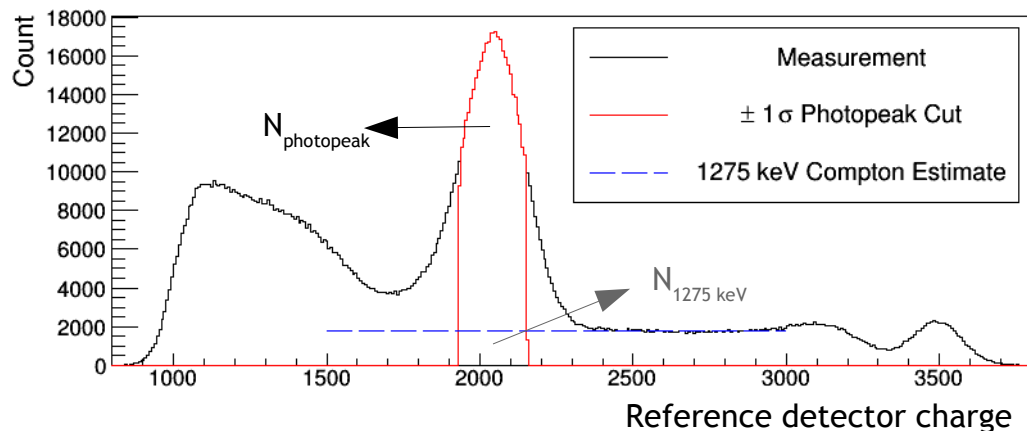
Detection efficiency estimation

- Geometrical collimation of coincidences - reference detector further away from the source

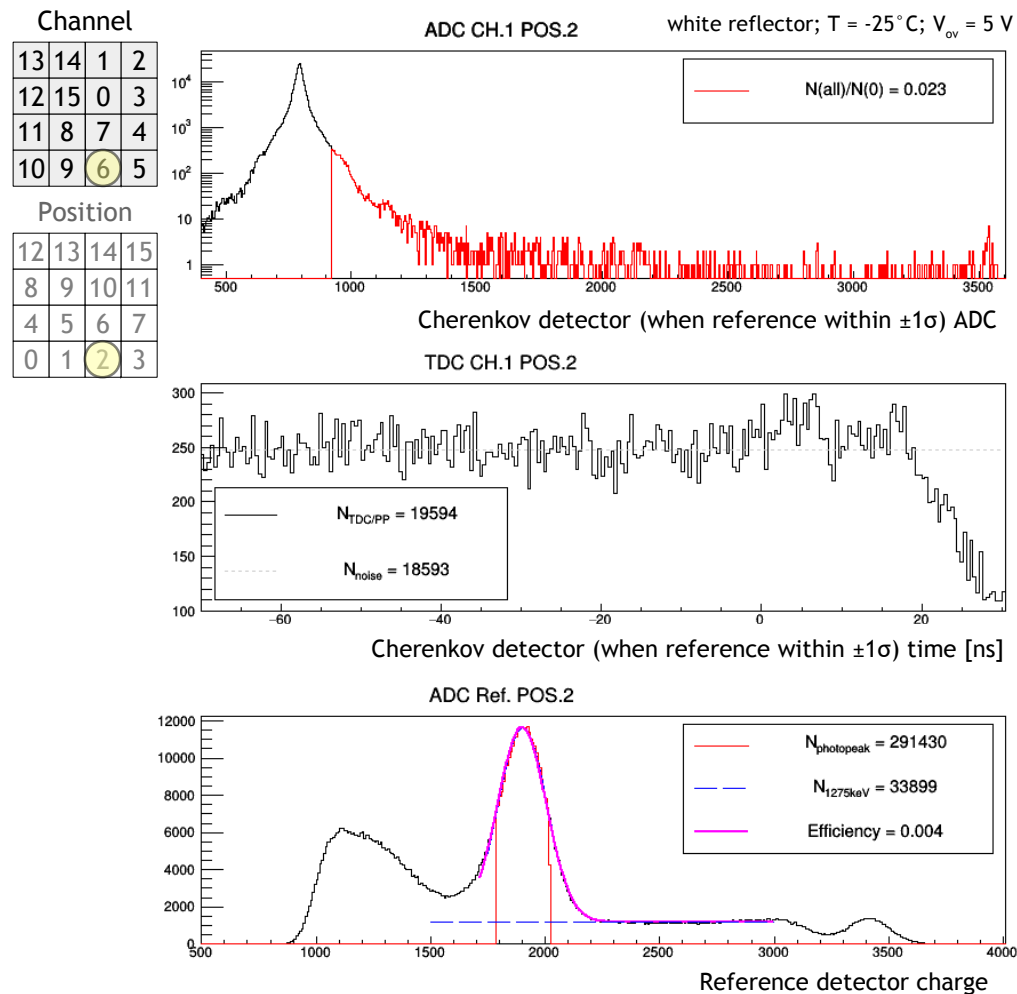
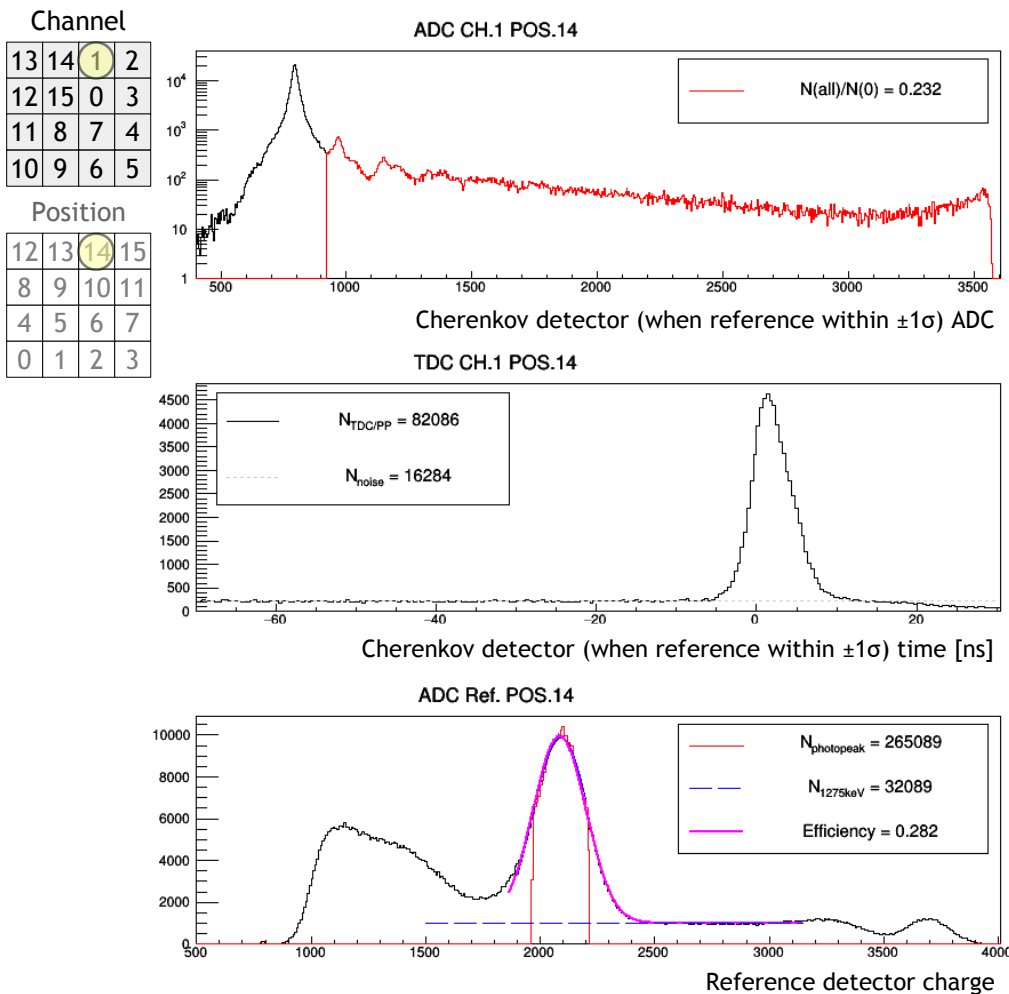


- When the reference scintillation detector is hit with one 511 keV γ , the other annihilation γ hits the Cherenkov detector
 - reference detector hit: event cut within $\pm 1\sigma$ of 511 keV photopeak
 - corrected for estimated 1275 keV γ (^{22}Na) Compton contribution
 - Cherenkov detector hit: TDC within 30 ns
 - corrected for noise, estimated from constant fit in off-time window

$$\text{Efficiency} = \frac{N_{\text{TDC/PP}} - N_{\text{noise}}}{N_{\text{photopeak}} - N_{1275\text{ keV}}}$$



Results: source position on channel / off channel

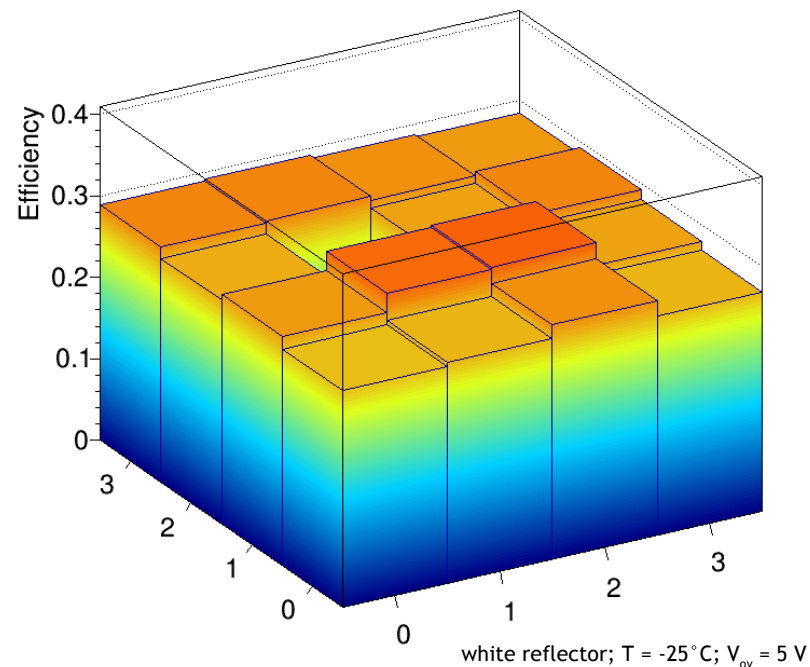
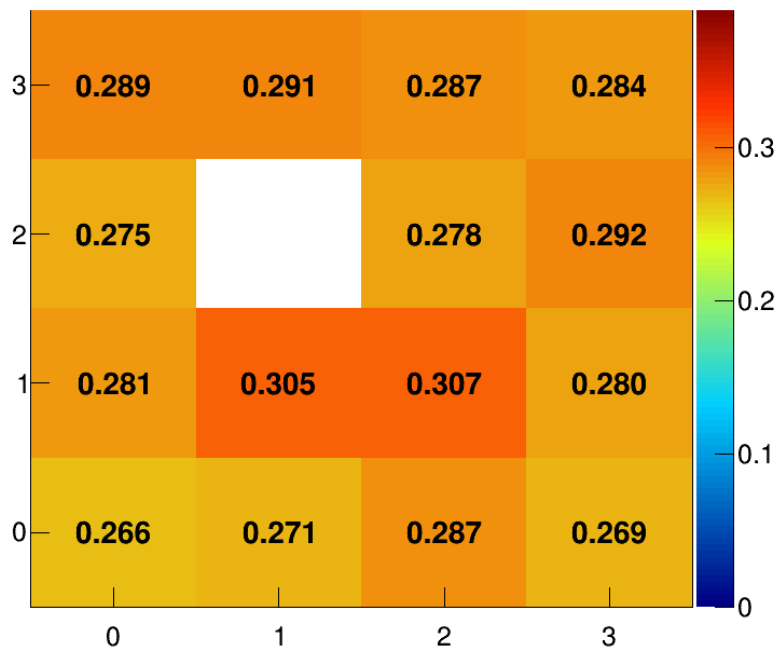


Results: efficiency map

- Efficiency of each channel when collimated with the source
 - average = 28.4% (previous single ch. result ~ 25% - 30%)

Channel			
13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5

Position			
12	13	14	15
8	9	10	11
4	5	6	7
0	1	2	3



white reflector; $T = -25^{\circ}\text{C}$; $V_{ov} = 5\text{ V}$

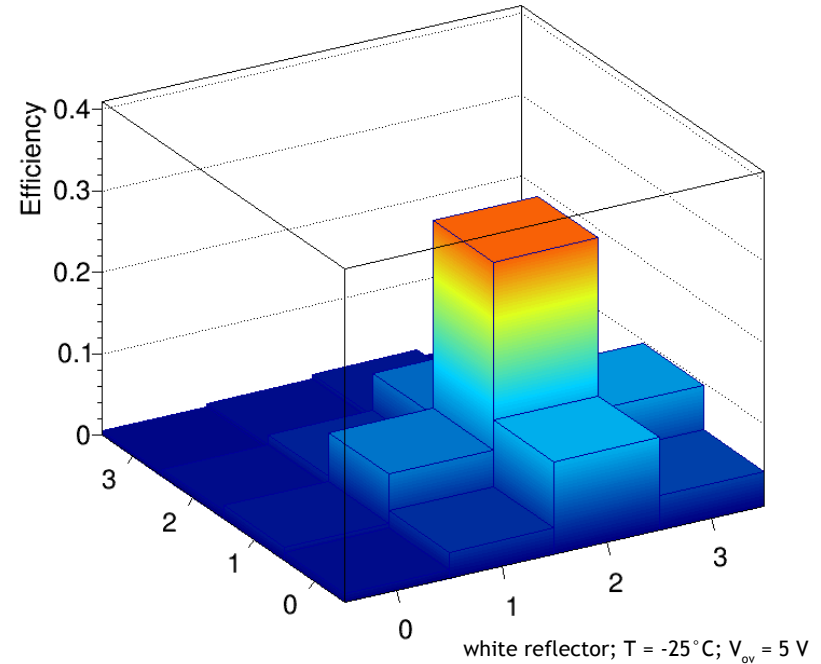
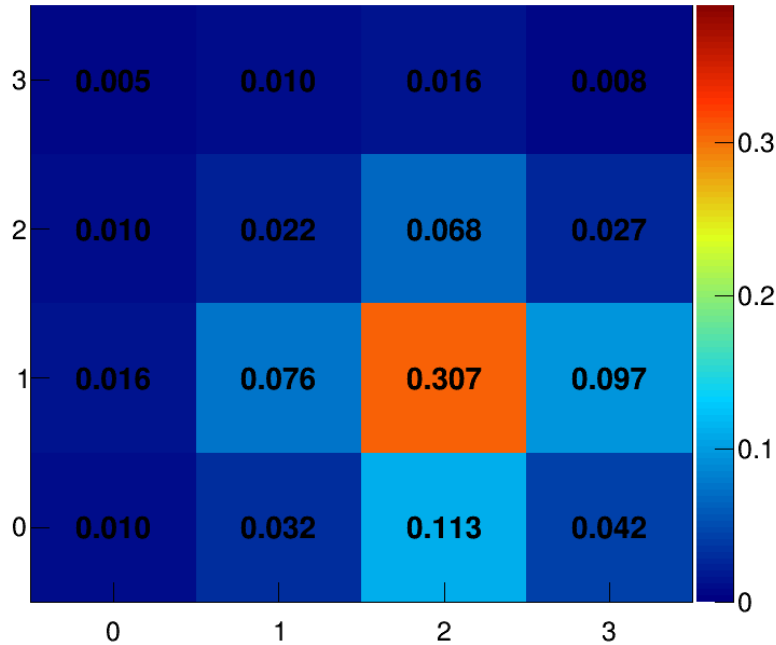
* ch.0 next to ground - more noisy; ch.15 TDC not connected

Results: cross talk

- Efficiency of channel 7, for all 16 source positions
 - nearest neighbors average 26% crosstalk
 - diagonal neighbors average 7% crosstalk
- Sources of crosstalk:
 - miss-collimation
 - optical leakage between channels
 - Compton scattering

Channel			
13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5

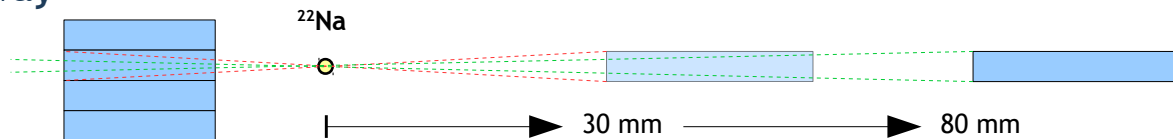
Position			
12	13	14	15
8	9	10	11
4	5	6	7
0	1	2	3



Results: cross talk - miss-collimation

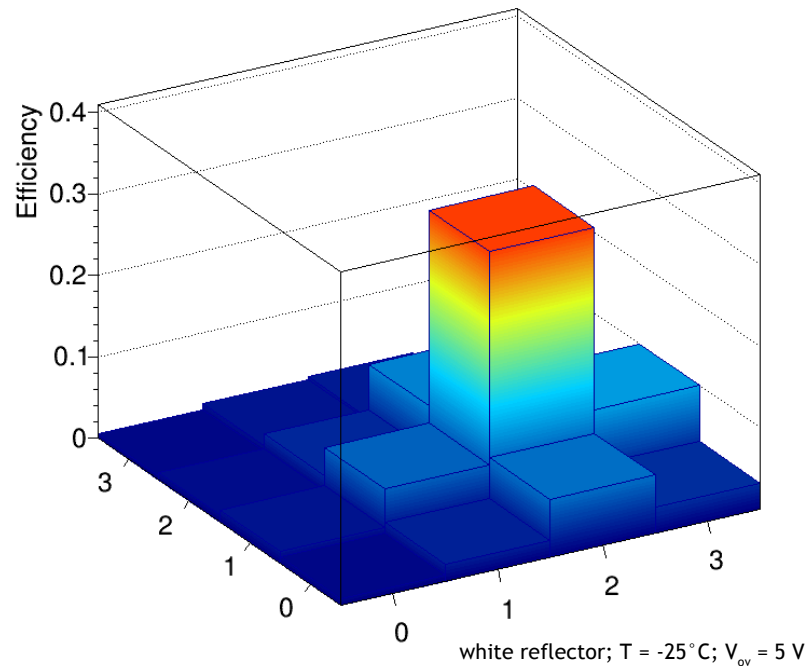
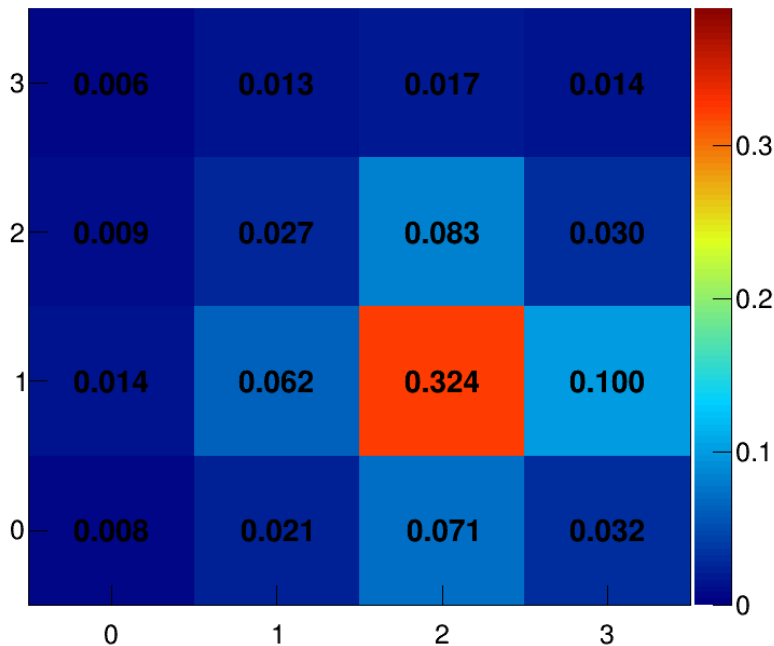
- When reference detector moved further away

- nearest neighbors average 22% crosstalk
- diagonal neighbors average 5% crosstalk



Channel			
13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5

Position			
12	13	14	15
8	9	10	11
4	5	6	7
0	1	2	3

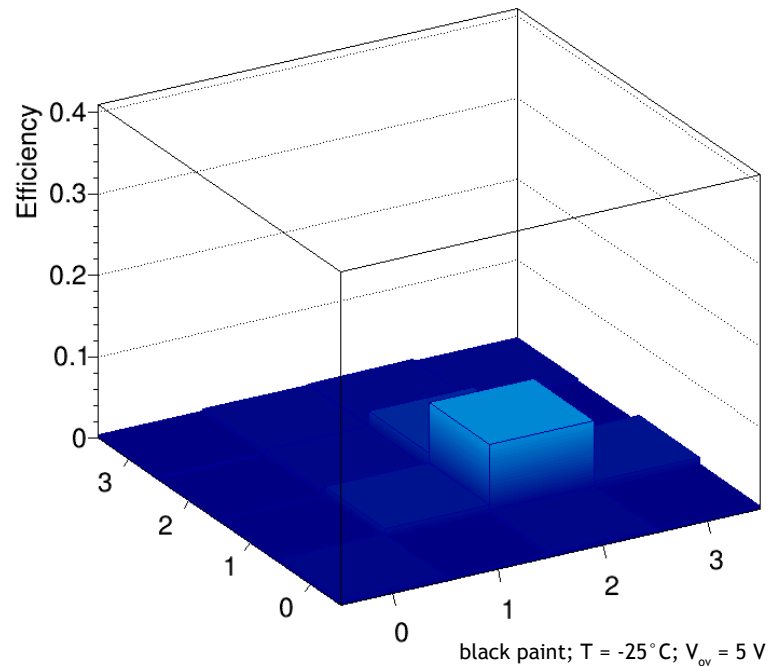
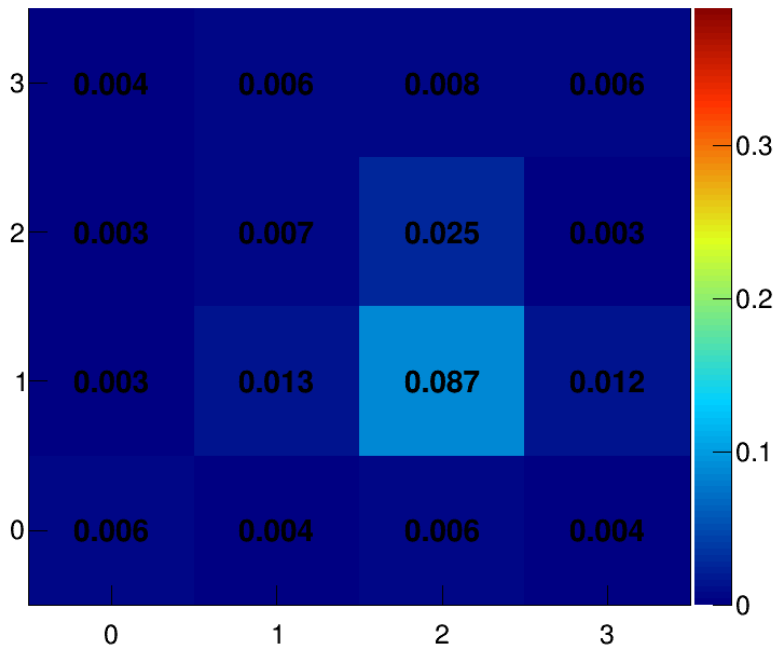


Results: cross talk - optical leakage between channels

- Crystal array **black painted** instead of white reflector
 - nearest neighbors average 11% crosstalk
 - diagonal neighbors average 0% crosstalk

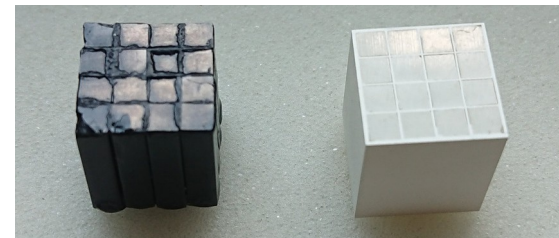
Channel			
13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5

Position			
12	13	14	15
8	9	10	11
4	5	6	7
0	1	2	3



Results: efficiency map for black painted array

- Efficiency of each channel when collimated with the source
 - average = 6.9% (previous single ch. result ~ 5% - 8%)
 - much less homogeneous results
 - lower quality of crystal array assembly

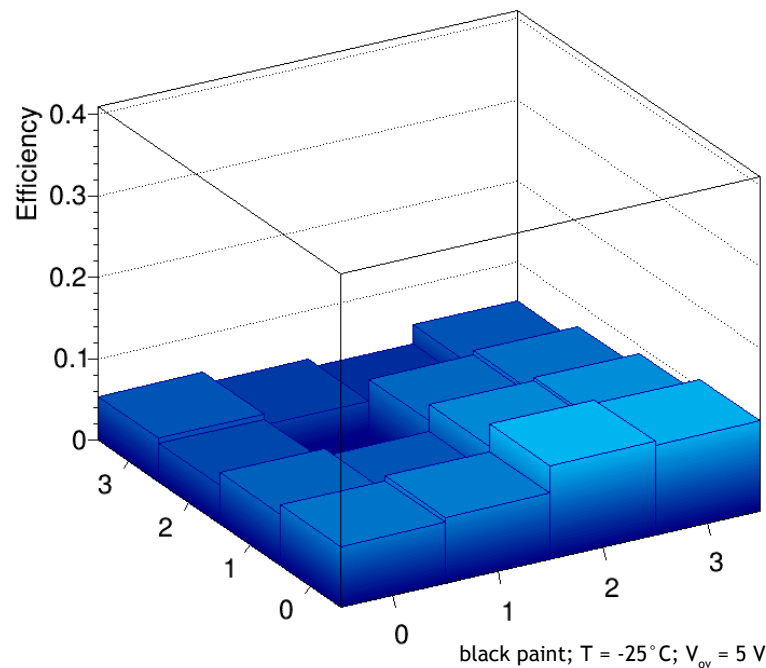
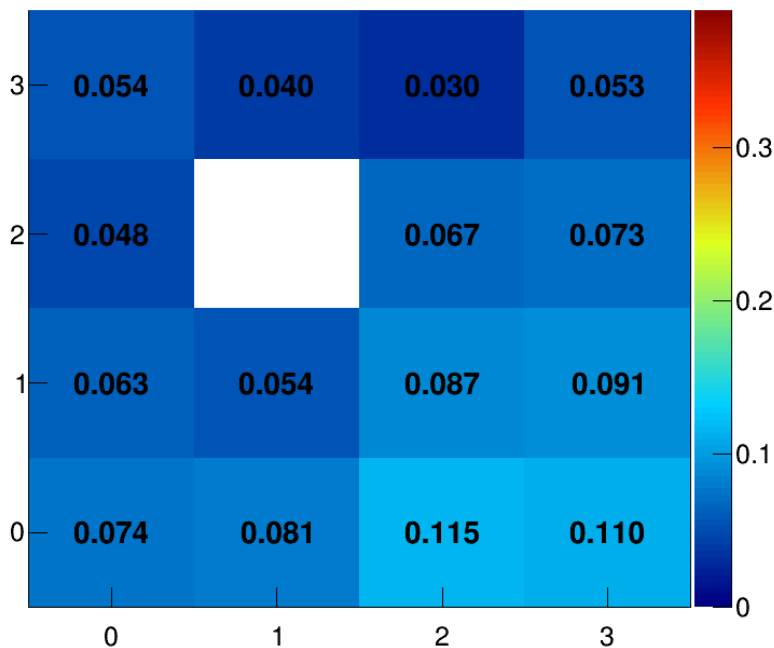


Channel

13	14	1	2
12	15	0	3
11	8	7	4
10	9	6	5

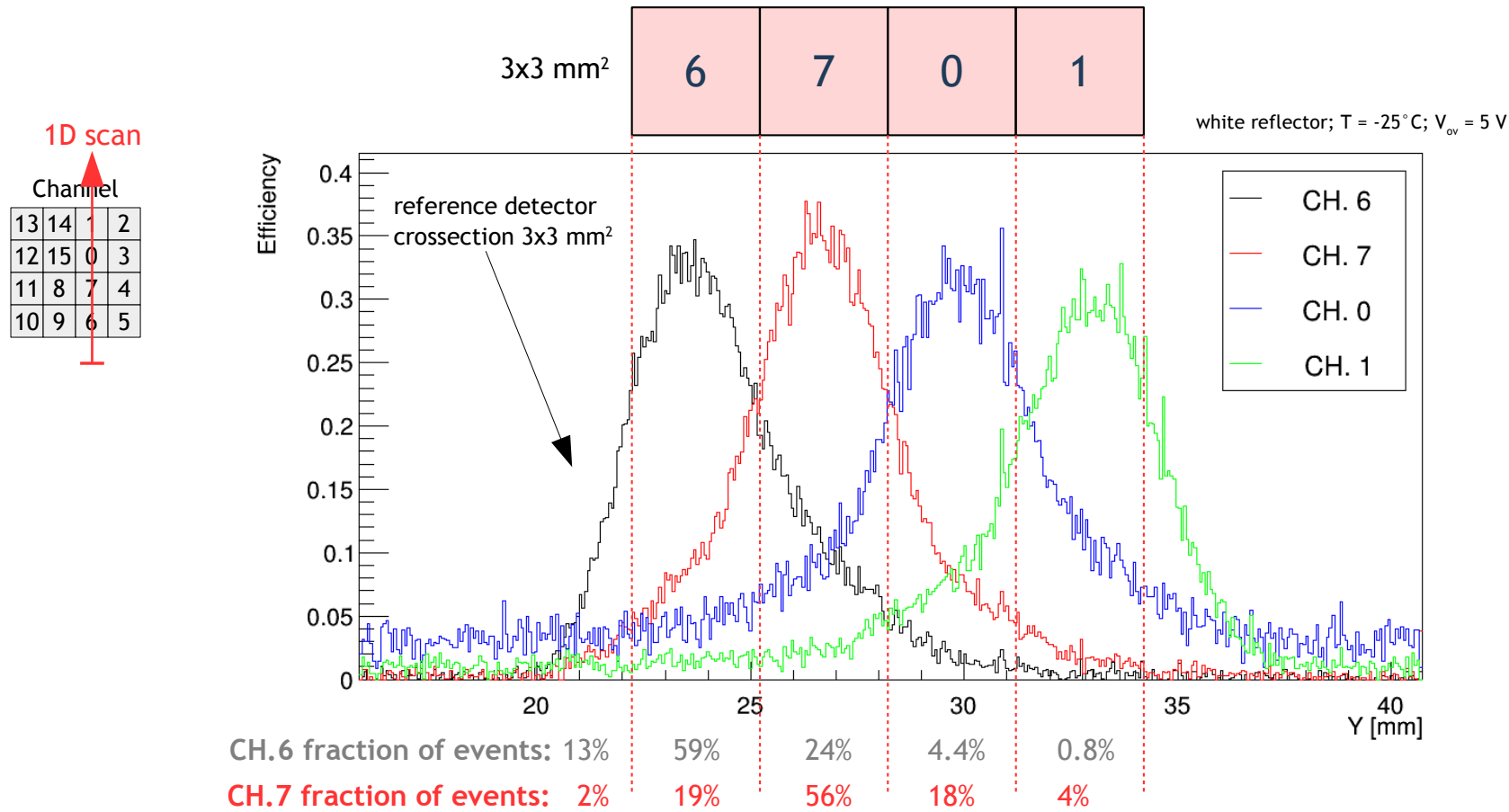
Position

12	13	14	15
8	9	10	11
4	5	6	7
0	1	2	3



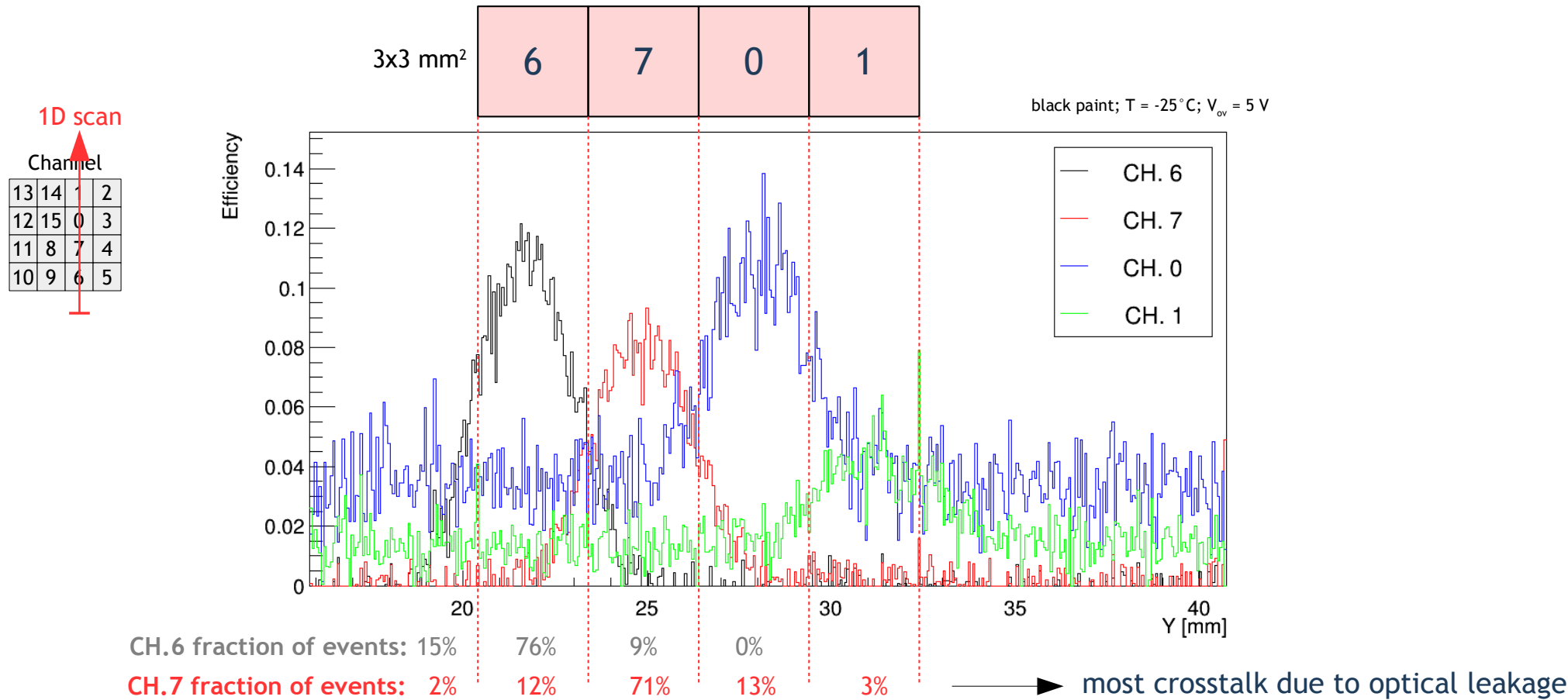
Results: cross talk

- Source scanned over one column of SiPM array



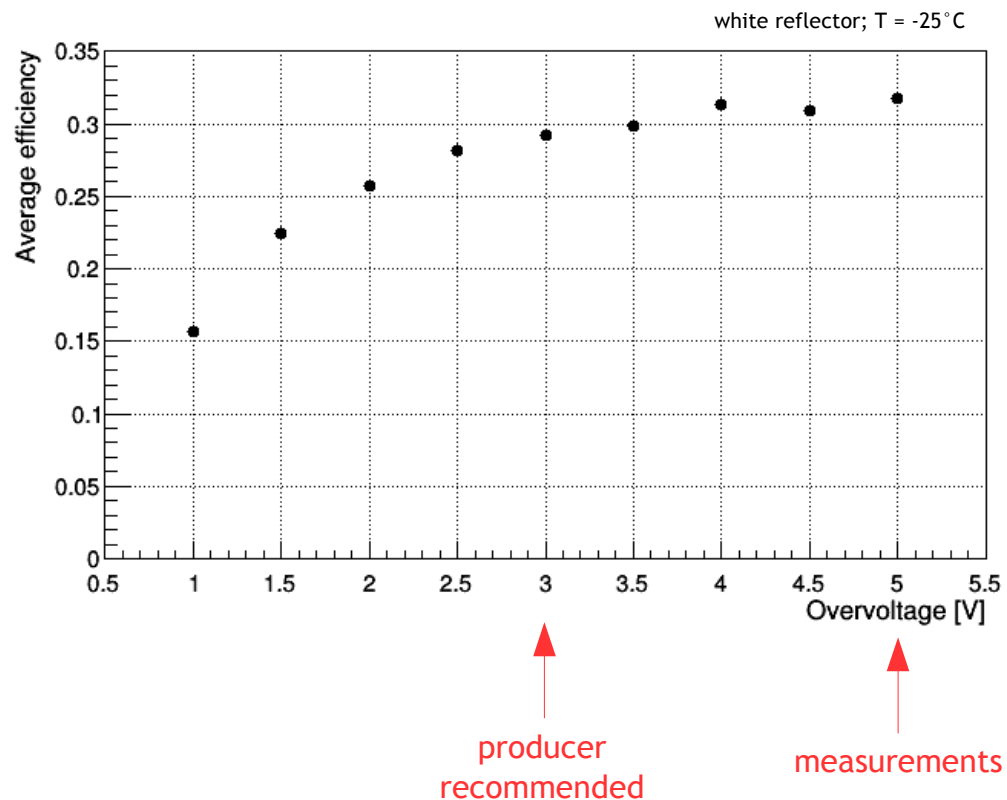
Results: cross talk

- Source scanned over one column of SiPM array - black painted array



Results: efficiency vs. SiPM overvoltage

- Average efficiency over all (15 connected) channels



Summary

- Use of Cherenkov light in PET
 - TOF resolution <100 ps FWHM (limited efficiency)
 - efficiency 30% single side (limited TOF resolution)
- Low cost of PbF_2
 - reduce cost PET of scanners (limited TOF, but still competitive performance)
 - total-body PET scanners
- 16 channel PET module
 - 4x4 array of $3 \times 3 \text{ mm}^2$
 - PbF_2 Cherenkov radiator + SiPM photodetector
 - efficiency 28% single side
 - good uniformity
 - optical crosstalk between channels should be reduced
- Next steps
 - 2-4 modules in coincidence
 - study effects of Compton events

